

1 Symmetries in muscle torques and landing kinematics are associated with maintenance of sports
2 participation at five to ten years after ACL reconstruction in young men

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Abstract

Background: Long-term maintenance of sports participation is important for young adults men undergoing ACL reconstruction. Identifying biomechanical characteristics in patients who achieve this goal can assist in elaborating rehabilitation programs and in identifying successful recovery but this has rarely been investigated.

Purpose: To test the association between maintenance of sports participation at 5-to-10 years after ACL reconstruction and measures of force production and landing biomechanics in adult men.

Study Design: Case series. Level of evidence, 4

Methods: Thirty men with isolated ACL reconstruction were examined. At 5-to-10 year follow-up, associations were tested between reported outcomes of sports maintenance and objective biomechanical measures. The biomechanical tests included isokinetic knee torques and lower limb kinetics and kinematics during landing tasks. Measurements for each limb were conducted separately and side-to-side symmetry indices (SI) were calculated.

Subgroups included SI higher than (+)10% (i.e. extreme positive), SI lower than (-)10% (i.e. extreme negative), and SI between -10% and +10% (i.e. symmetric).

Results: At follow-up, concentric knee torques in the operated limb correlated with Tegner and Marx scores ($r = 0.42$ to 0.47 , $p < 0.05$). Regarding SI of knee torques, highest Tegner, Marx and KOOS scores were associated with symmetric as opposed to patients with extreme positive or extreme negative SI ($p < 0.05$). As for landing kinematics, Tegner score negatively correlated with knee range of motion (ROM) in the operated limb ($r = -0.38$, $p < 0.05$). With regard to SI, hip and knee ROM correlated with Tegner, IKDC and KOOS scores ($r = 0.41$ to 0.51 , $p < 0.05$). Specifically, highest sports participation levels were

43 associated with achieving symmetric hip and knee ROM but also with extreme positive SI
44 as opposed to patients with extreme negative SI ($p < 0.03$) indicating substantially higher
45 ROM in the uninjured limb compared to the operated limb.

46 Conclusion: At 5-to-10 years after ACL reconstruction, maintenance of sports participation
47 is associated with symmetric side-to-side concentric knee torques and with producing
48 greater attenuation of hip and knee ROM during drop jump landing in the operated limb.
49 Therefore, eccentric load programs which can improve attenuation phase kinematics during
50 landing tasks may be valuable in addition to concentric training and facilitate enhanced
51 long-term outcomes.

52 Keywords: ACL reconstruction; drop jump test; single-legged landing test; isokinetic
53 strength test; sports participation

54 **What is known about the subject:** Previous-researchers have demonstrated the value of
55 identifying asymmetries in hip and knee kinematics during the early phases of rehabilitation
56 after ACL reconstruction. Symmetry indices of knee extensors and flexors torques were also
57 suggested fundamental to guide decision-making during the first and second years after
58 surgery. Focusing on the first two years after surgery is not surprising since return to sports
59 is the primary goal of surgery and therefore the primary interest of many investigators. Less
60 focus is applied in the literature to maintaining sports activities at more than 5 years after
61 surgery. It is unclear whether and which asymmetries in lower limb biomechanics could be
62 identified at this time frame and associated with achieving this target.

63 **What this study adds to existing knowledge:** The current study is unique in that it
64 explores knee torques and lower limb biomechanics long after ACL reconstruction in a
65 specific population of young adult men and identifies specific associations between lower

66 limb biomechanical characteristics and level of maintenance of sports participation. The
67 findings provided can potentially assist in decision-making junctions long after surgery.

68 **Introduction**

69 Returning to sport with the reestablishment of normal knee biomechanics is the primary
70 goal of anterior cruciate ligament (ACL) reconstruction surgery. Following that,
71 maintenance of sports activities throughout the years becomes a second important target,
72 particularly for those who undergo surgery at a relatively young age. This target is related to
73 a multifactorial process involving complex neuromuscular recovery among other factors
74 which evolve over the years [17]. One suggested strategy to improve decision making for
75 young athletes throughout the early recovery and later during the sports maintenance
76 process is by integrating subjective measures (i.e. patient reported outcome scales) with
77 objective biomechanical measures that assess knee function [7]. Until today however, there
78 has been limited evidence to support clear associations between objective measures of knee
79 function in sports-related tasks and the achievement of returning to sports alongside long-
80 term maintenance of sports activities [6]. Further information in this respect can therefore be
81 valuable. In addition, noticeable limitations of study designs related to this subject can be
82 appreciated. These include relying primarily on shorter than 2 years follow-up assessments
83 which miss the time-frame of long-term maintenance of activities and on heterogeneous
84 study populations of mixed graft sources and multiple age groups or combining both sexes
85 for a reported outcome [8, 15, 21]. Because knee function after ACL reconstruction is
86 affected by patient age [16, 18], duration of follow-up, graft source [32, 33, 37, 41], and sex
87 [2, 8, 13, 19, 30, 37, 40], greater specificity of patient demographics and surgical procedure
88 was recommended [21] and longer follow-up is required in order to evaluate function
89 specifically during the maintenance phase after surgery. Furthermore, since ACL
90 reconstruction is particularly justifiable in the young adult age group (i.e. 18-35 years) [36],

91 5-to-10 year follow-up could represent optimal time frame for assessing maintenance of
92 sports activities beyond the short-term recovery. This is because longer follow-up may
93 further subject the outcomes to changes in life style for other reasons than the knee injury or
94 to potential progression of other health-related problems which may confound the
95 interpretation of maintenance of sports activities in relation to the knee recovery [23, 29,
96 39]. The purpose of the current study was therefore to test the association between
97 maintenance of sports participation at 5-to-10 years after ACL reconstruction and measures
98 of force production and landing mechanics in young adult men. Based on a meta-analysis
99 that showed altered lower limb kinetics and kinematics at more than 3 years after ACL
100 reconstruction [10], it was hypothesized that at more than 5 years after surgery
101 biomechanical abnormalities through the ankle, knee, and hip joints, could still be identified
102 and that specific associations between objective biomechanical measures and measures of
103 maintaining sports activities could be determined.

104 **Materials and Methods**

105 Patients who underwent autologous quadrupled Gracilis-Semitendinosus ACL
106 reconstruction between 2004 and 2010 at a single arthroscopy unit were identified. The
107 surgery was performed in all patients using similar principles of trans-tibial femoral tunnel
108 drilling technique. Inclusion criteria for this study were: (1) male sex; (2) ACL tear which
109 occurred during sport activity only; (3) age at surgery 18 to 35 years; (4) isolated ACL
110 reconstruction without concomitant knee ligament reconstruction; and (5) 5-to-10 year
111 follow-up. Exclusion criteria were: (1) contra-lateral ACL tear; (2) revision ACL
112 reconstruction that was performed during the follow-up period or MRI-documented ACL
113 graft tear with functional instability awaiting revision; and (3) other significant lower limb
114 injury, surgery, or deformity which could affect lower limb function. In accordance with
115 these criteria, 55 patients were eligible and available for latest clinical follow-up evaluations

116 and their outcomes and outcomes-associated risk factors were published in a separate
117 manuscript [12]. Of these 55 patients, 30 volunteered to participate in the current study
118 which involved further tests in a biomechanical laboratory set-up. To assess maintenance of
119 sports activities, Tegner [38] and Marx [24] scores were used to indicate level of activity,
120 while the International Knee Documentation Committee (IKDC)-subjective score [3] and
121 the Knee Osteoarthritis and Outcome Sub-scores (KOOS) [35] were used to indicate
122 subjective knee function. Clinical evaluation of knee laxity was performed using side-to-
123 side difference by KT-1000 knee arthrometer device (MEDmetric Corp, San Diego, CA)
124 while the knee was in 25° flexion and under anteriorly-directed 30lbs of force. All KT-1000
125 measurements were performed by one independent investigator (***) that was not involved
126 in the index surgery. Four objective tests to assess knee biomechanics were performed in a
127 biomechanical laboratory by another independent investigator (***) which was not involved
128 in the index surgery and was blinded to the KT-1000 measurements or the patient reported
129 outcome scores. These included: (1) isokinetic strength tests of knee flexors and extensors,
130 (2) single-legged landing test, (3) double-legged drop jump test, and (4) single-legged hop
131 test for distance.

132 Biodex system 3 isokinetic dynamometer (Biodex Medical Systems Inc., Shirley, NY, USA)
133 was used to measure knee flexors and extensors maximal torque and work at 180°/sec. The
134 testing was performed in a seated position, with the hip at 110° flexion angle and the knee at
135 90° flexion angle as a comfortable starting position. The participant was secured to the chair
136 by two straps across the chest and a single strap at the abdomen and distal thigh of the tested
137 limb in order to minimize compensations. Knee range of motion (ROM) was set at 90⁰ with
138 0⁰ indicating full extension. Prior to testing, correction for gravity of the tested limb was
139 performed, and several warm-up repetitions were completed. These included 3 sub-maximal
140 repetitions and 2 maximal repetitions at 180°/sec. All participants started the test with the

141 healthy uninjured knee tested before the operated knee. During the test, the participant was
142 encouraged to perform 5 repetitions in maximal torque of knee flexion and extension at
143 180°/sec. Outcome measure of the test was peak flexors and extensors torque [N*m/Kg].

144 For the single-legged landing test and double-legged drop jump test the following
145 biomechanical model was used for movement analysis: Twenty one photo-reflective
146 markers were placed at anatomical landmarks on each lower extremity from foot to pelvis
147 level. Location of markers was in accordance with standard plug-in gait protocol (User
148 Manual, Vicon Motion Systems, Ltd., Oxford, UK). A Knee Alignment Device (KAD) was
149 mounted on each knee at the beginning of each examination for the purpose of segments
150 alignment setup at the neutral standing position during a static trial and was then removed
151 prior to beginning the dynamic tests. In both tests the participant landed on a force plate
152 (Kistler Group, Winterthur, Switzerland) sampled at 960 Hz. A six camera optical
153 stereometric system (Vicon Motion Systems, Ltd., Oxford, UK), sampling at 240 Hz, was
154 used to track lower extremity motions. Data were sampled using NEXUS 1.7.1 program
155 with Woltring filter for filling gaps and Butterworth fourth order filter with cut off
156 frequency of 6 Hz built in the program, and reports were processed with Polygon 3.5.1
157 software (Vicon Motion Systems, Ltd., Oxford, UK).

158 The single-legged landing test was performed in accordance with previous investigation [5]
159 as follows: The patient was standing on a 21-cm height step located 6-cm in front of the
160 force plate. The subject's initial position was with both feet on the step facing the force
161 plate. Subjects were instructed to place the hands on the waist. The subject stepped forward
162 with the test leg, and dropped from the step, landing on the force plate on the test leg only.
163 Participants were instructed to stabilize as quickly as possible. After the landing, the subject
164 remained on the force plate for three seconds at the described position. The performance
165 was disqualified and performed again if the opposite leg also touched the ground. Between

166 the performances the patient rested 30 seconds. This test was performed 3 times for each
167 leg. The following measures were extracted from this test: (1) Time to stability [seconds];
168 and (2) Peak vertical ground reaction forces (GRF)/BW [N/Kg]. The beginning of the
169 landing phase was defined as the time that the force platform signal reached 20N. The
170 moment of stability was defined in accordance with previous investigators [5] as the time
171 from which the moving average signal did not exceed 25% of the average of standard
172 deviation of the whole series mean. Results are reported based on the average of the three
173 trials.

174 The drop jump test was performed in accordance with previous investigations [25, 31] as
175 follows: The patient was standing on a 21-cm height step located 6-cm in front of the force
176 plate. The subject's initial position was with both feet on the step facing the force plate.
177 Subjects were instructed to place the hands on the waist. The patient dropped off the box,
178 landed with each foot onto a separate force platform and immediately executed a maximal
179 effort vertical jump. The eccentric phase of the drop landing was defined as the duration
180 from time that the force platform signal reached 20N to the lowest vertical height of the line
181 connecting the right and left anterior superior iliac spine markers. The following measures
182 were extracted for each limb during the eccentric phase of the drop jump test: (1) Peak
183 support moment [42], computed as the momentary highest summation of sagittal torques of
184 hip extension, knee extension, and ankle plantar flexion [N*m/Kg]; and (2) ROM in the
185 sagittal plane at the ankle, knee and hip joints [°]. ROM was defined as the difference
186 between maximal flexion and maximal extension during the eccentric phase. Total ROM of
187 the lower limb during the eccentric phase of the drop jump was computed as the summation
188 of the ankle, knee and hip ROMs. Results are reported as average of all trials.

189 The Single-legged hop test for distance was performed with take-off and landing on the
190 same limb as described [28]. The distance was measured bilaterally. The longest hop of
191 three trials was selected for analysis.

192 The symmetry index (SI) for all biomechanical measures was calculated in accordance with
193 accepted formula used to indicate asymmetries between the limbs in different variables of
194 gait [34] as follows: $SI[\%] = 2 \cdot (X_n - X_i) / (X_n + X_i) \cdot 100$, where "X_n" indicates the value of
195 variable in the uninjured side, and "X_i" indicates the value of variable in the injured side.
196 Perfect symmetry is achieved when "SI" equals zero.

197 The study was approved by the institutional review board and each participant signed
198 informed consent.

199 Statistical analysis

200 The study sample size was in accordance with previous investigations that evaluated hip and
201 knee landing kinetics and kinematics after ACL reconstruction. These referred to sample
202 sizes of between 11 and 35 patients [21]. Intraclass correlation coefficients (ICCs) were
203 computed to estimate the reliability of the biomechanical measures. Associations between
204 the subjective measures of ongoing sports participation at 5-to-10 year follow-up and the
205 objective measures of muscle strength and landing biomechanics were analyzed by means
206 of Pearson's product-moment correlations. In addition, due to large standard deviations
207 observed in most biomechanical measures among the participants despite symmetric mean
208 values, subgroup analysis was added to assess whether extreme asymmetry in any of the
209 objective biomechanical variables was associated with reported outcome scores of sports
210 participation. For this purpose, 3 subgroups were defined in relation to the symmetry indices
211 (SI) of the biomechanical variable as follows: (1) subgroup of patients with extreme positive
212 SI, i.e. SI higher than (+)10% (uninjured limb was characterized by substantial higher value

213 of the biomechanical variable compared to operated limb); (2) subgroup of patients with
214 extreme negative SI, i.e. SI lower than (-)10% (operated limb was characterized by
215 substantial higher value of the biomechanical variable compared to uninjured limb); and (3)
216 subgroup of patients with almost perfect side-to-side symmetry, i.e. SI between (-10%) and
217 (+10%). With each sports participation outcome score as a dependent variable, a series of
218 one-way ANOVAs were applied for each biomechanical variable in order to compare the
219 means among the three subgroups. In case of a significant main effect a Tukey HSD
220 procedure was used for post hoc comparisons among the means. Level of significance was
221 set at 0.05. SPSS Software version 25 was used for data analysis.

222 **Results**

223 Mean Tegner activity level before the injury was 8.0 ± 1.4 (range 7-10), supportive that the
224 studied sample represented ACL reconstruction in active population in terms of cutting-
225 pivoting sports. Table 1 presents the patient reported outcome scores at 5-to-10 years after
226 surgery.

227 Table 1: Descriptive statistics of the patient activity reported outcomes

Reported outcome scale	Mean \pm SD
Tegner activity level	6.0 ± 2.3
Marx activity level	6.4 ± 5.4
IKDC-subjective	83.3 ± 13.2
KOOS-Knee symptoms	82.9 ± 11.3
KOOS-Pain	87.8 ± 12.7
KOOS-ADL	94.5 ± 9.3
KOOS-Sports	76.8 ± 20.8
KOOS-QOL	62.0 ± 22.2

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229 Mean activity level scores indicated that patients were still maintaining moderately intense
230 sports activities. Among the reported functional outcomes scales, the lowest scores were

231 represented by KOOS-sports and KOOS-QOL sub-scores which also displayed the largest
 232 score variability.

233 Table 2 presents descriptive statistics of all biomechanical measures in the operated limb
 234 and in the contralateral uninjured limb.

235 Table 2: Descriptive statistics of the biomechanical measures (mean \pm SD)

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Variable	ACLR limb	Contralateral limb	Symmetry Index (%)
Knee extension isokinetic peak torque (N*m/kg)	1.73 \pm 0.4	1.85 \pm 0.4	6.8 \pm 21.5
Knee flexion isokinetic peak torque (N*m/kg)	0.88 \pm 0.2	0.90 \pm 0.2	2.4 \pm 18.8
Single-legged landing time to stability (sec)	1.25 \pm 0.1	1.25 \pm 0.1	0.3 \pm 6.3
Single-legged landing peak GRF/BW (N/kg)	39.3 \pm 8.4	40.1 \pm 9.8	1.7 \pm 11.5
Drop jump - peak support moment/BW (N*m/kg)	4.75 \pm 1.5	4.69 \pm 1.6	-1.6 \pm 22.7
Drop jump – hip torque at peak support moment (N*m/kg)	1.78 \pm 0.52	1.45 \pm 0.61	-16.9 \pm 47.1
Drop jump – knee torque at peak support moment (N*m/kg)	1.59 \pm 0.80	1.67 \pm 0.83	5.1 \pm 42.3
Drop jump – ankle torque at peak support moment (N*m/kg)	1.38 \pm 0.55	1.57 \pm 0.71	5.9 \pm 24.5
Drop jump - sagittal hip ROM ($^{\circ}$)	31.3 \pm 14.5	30.7 \pm 13.7	-3.3 \pm 18.0
Drop jump - sagittal knee ROM ($^{\circ}$)	47.5 \pm 13.3	49.1 \pm 13.7	3.6 \pm 19.4
Drop jump - sagittal ankle ROM ($^{\circ}$)	39.2 \pm 18.6	41.9 \pm 16.7	9.1 \pm 42.8
Drop jump - sagittal total ROM (hip + knee + ankle) ($^{\circ}$)	118.0 \pm 32.4	121.7 \pm 35.5	2.6 \pm 24.7
Single-legged hop for distance (m)	1.79 \pm 0.3	1.84 \pm 0.2	1.6 \pm 6.9

237 Positive symmetry index indicates a higher value of the measured variable in the
 238 contralateral uninjured limb and negative symmetry index indicates a higher value of the
 239 measured variable in the operated limb. In all measures, except hip torque component of the
 240 overall peak support moment (defined as hip torque at peak support moment) during drop
 241 jump landing, mean side-to-side symmetry indices were within $\pm 10\%$ but large standard
 242 deviations suggested high variability among subjects in almost all biomechanical measures
 243 tested.

244 Tables 3 and 4 present bi-variate correlation coefficients between Tegner, Marx, IKDC and
 245 KOOS scores and each biomechanical measure.

246 Table 3: Bi-variate correlation coefficients relating to the contralateral uninjured limb (CL),
 247 the operated limb (ACLR), and the symmetry index between the limbs (SI) for the Tegner,
 248 Marx, and IKDC scores

Variable	Tegner preinjury [CL; ACLR; SI]	Tegner FU [CL; ACLR; SI]	Marx FU [CL; ACLR; SI]	IKDC [CL; ACLR; SI]
Peak knee extensors torque at 180°*sec ⁻¹	0.44** ; 0.54** ; -0.15	0.33; 0.46* ; -0.21	0.44* ; 0.47** ; -0.09	-0.06; 0.15; -0.29
Peak knee flexors torque at 180°*sec ⁻¹	0.52** ; 0.53** ; 0.03	0.31; 0.42* ; -0.13	0.29; 0.42* ; -0.15	-0.03; 0.14; -0.21
Single-legged landing - time to stability	0.05; 0.11; 0.05	0.13; -0.12; -0.31	0.17; -0.12; -0.37*	0.17; 0.05; -0.18
Single-legged landing - peak GRF/BW	0.35; 0.26; 0.23	0.33; 0.45* ; -0.17	0.14; 0.31; -0.17	0.13; 0.05; 0.18
DJ - peak support moment/BW	0.63** ; 0.57** ; 0.14	0.37; 0.38; -0.03	0.34; 0.37; -0.06	-0.20; -0.11; -0.24
DJ - hip torque at peak support moment	0.34; 0.32; -0.05	0.46* ; 0.47* ; -0.09	0.47* ; 0.51* ; -0.09	0.10; -0.03; -0.13
DJ - knee torque at peak support moment	0.64** ; 0.54** ; -0.08	0.17; 0.25; 0.14	0.14; 0.20; 0.15	-0.17; -0.02; 0.34
DJ - ankle torque at peak support moment	0.37; 0.44* ; 0.07	0.19; 0.20; -0.01	0.15; 0.22; 0.07	-0.41* ; -0.23; 0.29
DJ – hip sagittal ROM	-0.26; -0.41* ; 0.34	0.06; -0.12; 0.43*	0.11; -0.01; 0.27	0.40* ; 0.23; 0.51*
DJ – knee sagittal ROM	-0.33; -0.56** ; 0.39*	-0.17; -0.38* ; 0.33	-0.09; -0.25; 0.23	0.38* ; 0.06; 0.46*
DJ – ankle sagittal ROM	-0.24; -0.45* ; 0.25	-0.05; -0.32; 0.27	0.07; -0.25; 0.24	-0.05; -0.26; 0.24
DJ - total sagittal ROM [‡]	-0.35; -0.64** ; 0.33	-0.06; -0.38* ; 0.33	0.05; -0.24; 0.28	0.28; -0.01; 0.37
Single-legged hop test for distance	0.50** ; 0.65** ; 0.31	0.29; 0.33; -0.06	0.20; 0.31; 0.02	-0.09; 0.07; 0.34

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 250 Table 4: Bi-variate correlation coefficients relating to the contralateral uninjured limb (CL),
 251 the operated limb (ACLR), and the symmetry index between the limbs (SI) for the KOOS
 252 scores

Variable	KOOS KS [CL; ACLR; SI]	KOOS Pain [CL; ACLR; SI]	KOOS ADL [CL; ACLR; SI]	KOOS Sports [CL; ACLR; SI]	KOOS QOL [CL; ACLR; SI]
Peak knee extensors torque at 180°*sec ⁻¹	-0.07; 0.09; -0.20	-0.15; -0.11; -0.07	-0.05; 0.02; -0.11	0.02; 0.22; -0.27	0.10; 0.27; -0.24
Peak knee flexors torque at 180°*sec ⁻¹	-0.12; 0.03; -0.18	-0.21; 0.00; -0.29	-0.15; -0.09; -0.07	0.02; 0.20; -0.21	0.05; 0.28; -0.30
Single-legged landing - time to stability	0.13; 0.07; -0.07	0.09; 0.02; -0.11	0.23; 0.21; -0.05	0.19; 0.13; -0.10	-0.03; -0.12; -0.13
Single-legged landing - peak GRF/BW	-0.10; -0.10; -0.02	0.07; -0.06; 0.23	0.06; -0.06; 0.21	-0.01; -0.04; 0.02	0.04; 0.03; 0.07
DJ - peak support moment/BW	-0.26; -0.19; -0.24	-0.30; -0.23; -0.08	-0.18; -0.02; -0.26	-0.18; -0.08; -0.25	0.01; 0.00; -0.01
DJ - hip torque at peak support moment	-0.11; -0.25; -0.06	0.00; -0.15; -0.11	-0.19; -0.26; 0.02	0.04; 0.00; -0.03	0.26; 0.02; -0.29
DJ - knee torque at peak support moment	-0.25; -0.10; 0.35	-0.25; -0.10; 0.31	-0.01; 0.19; 0.38	-0.11; -0.05; 0.15	-0.05; 0.00; 0.14
DJ - ankle torque at peak support moment	-0.21; -0.12; 0.14	-0.45* ; -0.32; 0.13	-0.25; -0.08; 0.22	-0.36; -0.14; 0.33	-0.22; -0.03; 0.29
DJ – hip sagittal ROM	0.43* ; 0.35; 0.24	0.33; 0.27; 0.21	0.08; 0.01; 0.15	0.48** ; 0.33; 0.50**	0.36; 0.21; 0.48**
DJ – knee sagittal ROM	0.35; 0.19; 0.18	0.35; 0.14; 0.28	0.05; -0.10; 0.22	0.48** ; 0.19; 0.41*	0.44* ; 0.13; 0.46*
DJ – ankle sagittal ROM	0.20; -0.01; 0.15	-0.05; -0.25; 0.16	-0.03; -0.08; 0.06	0.11; -0.22; 0.29	0.04; -0.26; 0.29

DJ - total sagittal ROM [‡]	0.41* ; 0.23; 0.19	0.24; 0.05; 0.21	0.10; -0.08; 0.12	0.43* ; 0.10; 0.40*	0.40* ; 0.01; 0.43*
Single-legged hop test for distance	-0.13; -0.07; 0.09	-0.23; -0.01; 0.33	-0.07; 0.13; 0.40*	0.01; 0.14; 0.28	0.02; 0.15; 0.23

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At follow-up, Tegner and Marx activity level scores were positively correlated with concentric knee flexors and extensors peak torques and with hip torque at peak support moment in the operated limb during drop jump landing. Tegner scores were also positively correlated with single-legged peak GRF and negatively correlated with knee and total sagittal ROM in the operated limb during drop jump landing. In relation to symmetry indices, hip sagittal ROM symmetry index during drop jump landing positively correlated with Tegner score, and with IKDC, KOOS-Sports and KOOS-QOL sub-scores at follow-up, while knee sagittal ROM symmetry index during drop jump landing positively correlated with the latter three measures of sports maintenance. Preinjury Tegner scores significantly correlated with most unilateral biomechanical measures tested in the operated limb.

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Table 5 presents subgroup comparisons of the 3 symmetry indices categories of biomechanical measures that showed significant associations with ongoing sports participation scores. These included knee isokinetic muscle torques and hip and knee ROM during drop jump landing.

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Table 5: Comparisons of the activity outcome scores between subgroups of symmetry indices (SI) of knee torques and drop jump kinematics showing significant inter-relationships

Biomechanical measure	Activity reported outcome measure	SI subgroup			post hoc comparisons	p
		I SI <-10%	II SI ±10%	III SI >+10%		
Quad peak torque/BW	Marx latest FU	1.5 ± 1.9	9.0 ± 4.9	5.3 ± 5.3	I<II	0.025
	KOOS-knee symptoms	76.8 ± 9.6	89.1 ± 9.6	78.5 ± 10.8	I,III<II	0.024
Hams peak torque/BW	Tegner latest FU	6.0 ± 2.1	7.0 ± 2.2	4.7 ± 1.8	III<II	0.041

	Marx latest FU	6.7 ± 6.0	8.64 ± 5.3	3.1 ± 3.3	III<II	0.037
DJ hip sagittal ROM	IKDC-subjective	73.3 ± 10.5	85.5 ± 12.6	94.8 ± 5.1	I<II,III	0.006
	KOOS-knee symptoms	75.8 ± 7.8	84.5 ± 11.9	88.3 ± 10.0	I<II,III	0.073
	KOOS-sports	57.5 ± 15.5	84.5 ± 18.1	90.0 ± 9.1	I<II,III	0.001
	KOOS-QOL	41.5 ± 14.9	70.6 ± 18.4	72.0 ± 16.6	I<II,III	0.001
DJ knee sagittal ROM	KOOS-QOL	43.1 ± 17.5	63.1 ± 22.9	72.4 ± 12.4	I<III	0.027

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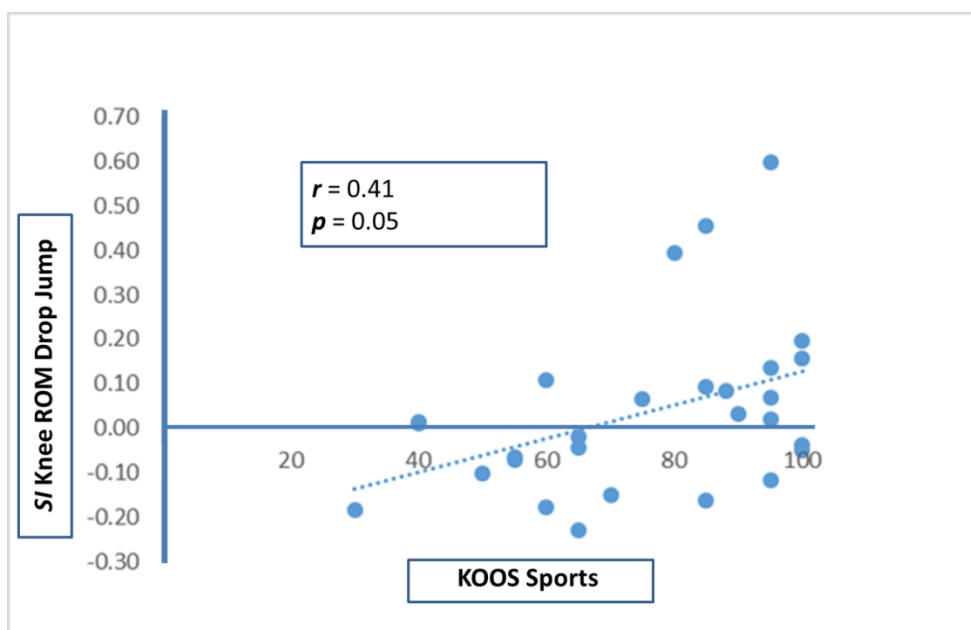
For isokinetic extensors and flexors knee torques, patients who reported the highest ongoing sports participation belonged to the mid-range subgroup of SI. These patients had close to perfect symmetry of extensors and flexors knee torque values. For hip and knee ROM during drop jump landing, patients who reported the highest ongoing sports participation belonged to the symmetric SI subgroup but also to the extreme positive SI subgroup (SI > +10%) which refers to patients with substantially higher hip and knee ROM in the uninjured limb compared to the operated limb during the drop jump landing.

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Figures 1 and 2 show on individual basis the correlations between knee and hip side-to-side SIs of ROM during drop jump landing and maintenance of sports participation as represented by KOOS-Sports sub-score.



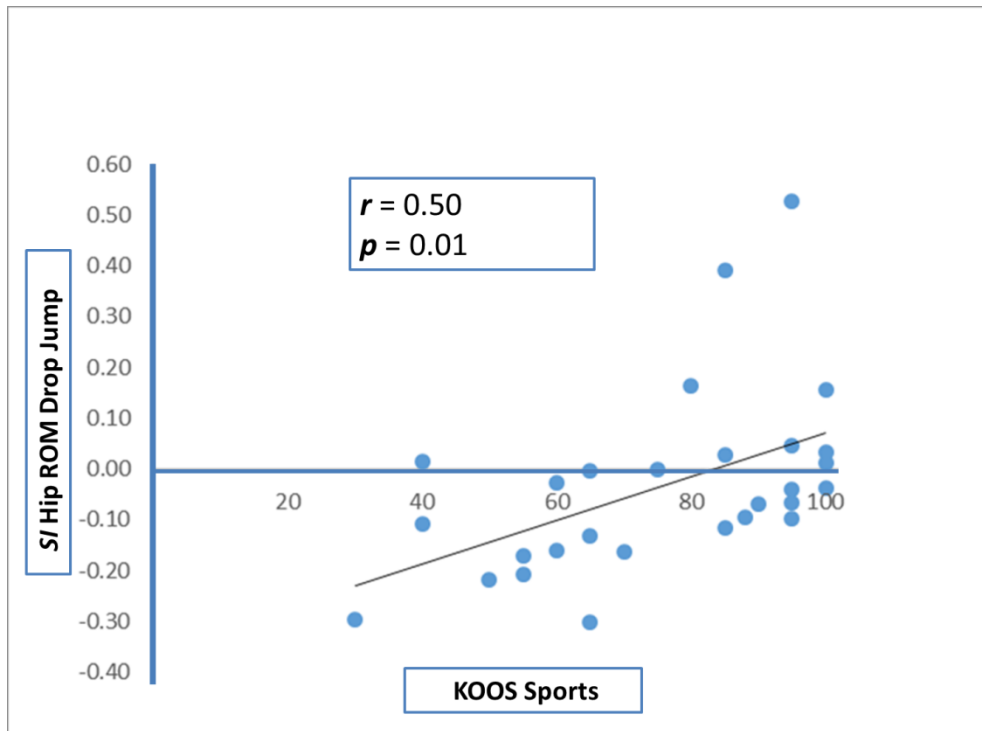
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Figure 1: Correlations between knee side-to-side SIs of ROM during drop jump landing and

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maintenance of sports participation as represented by KOOS-Sports sub-score



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Figure 2: Correlations between hip side-to-side SIs of ROM during drop jump landing and

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maintenance of sports participation as represented by KOOS-Sports sub-score

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Patients with higher scores (KOOS-Sports > 80) were characterized by positive SIs as

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opposed to patients with lower scores (KOOS-Sports < 80) which were characterized by

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negative SIs. This means greater attenuation of hip and knee ROM in the operated limb

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relative to the uninjured limb in more active patients.

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BMI was within normal range (mean 24.1 ± 2.2). KT side-to-side difference was 3.1 ± 2.2

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mm, and in 26 (87%) cases, the difference was ≤ 5 mm, which is considered "normal" or

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"nearly normal" [11]. This also supports the generalizability of the studied group in terms of

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surgical outcome and in accordance with others who evaluated similar graft source for ACL

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reconstruction at 7 years follow-up [22].

297 The ICCs were fair for the time to stability (ICC = 0.66 and 0.77 for the injured and
298 uninjured limb, respectively) and high for all other variables (ICC = 0.86-0.99).

299 **Discussion**

300 The present study was designed to test correlations between objective biomechanical
301 measures of force production and landing biomechanics versus maintenance of sports
302 participation at 5-to-10 years after ACL reconstruction. The most pronounced
303 biomechanical characteristics observed in patients who reported higher maintenance of
304 sports participation included: (1) symmetric concentric knee extensors and flexors torques,
305 (2) symmetric hip and knee ROM during drop jump landing, and (3) positive side-to-side
306 symmetry indices of hip and knee ROM indicating higher ROM in the uninjured limb
307 during drop jump landing. Inferior maintenance of sports participation was observed in
308 patients with inverse side-to-side relationships of hip and knee ROM where higher sagittal
309 motion appeared in the operated limb compared to the uninjured limb. In other words,
310 patients who reported higher activity scores have not only reestablished symmetric side-to-
311 side concentric knee extensors and flexors torques, but also showed improved hip and knee
312 sagittal plane motion attenuation immediately following ground contact which was
313 accompanied by higher GRFs and higher moments in the operated limb. Previous
314 investigators indicated the value of identifying asymmetries in hip and knee kinematics
315 during the early phases of the rehabilitation process after ACL reconstruction [25, 31]. The
316 current study shows that these asymmetries still remain valuable to distinguish between an
317 optimal and a suboptimal functional recovery and thus potentially guide decision-making
318 junctions long after surgery. These results are also consistent with previous investigators
319 who emphasized that the best functional outcome scores were observed in patients who
320 achieved symmetric knee range of motion during the rehabilitation phase after ACL
321 reconstruction [4]. Symmetry indices of isokinetic knee extensors and flexors torques were

322 also suggested fundamental to guide decision-making during the first and second years after
323 surgery [1, 9, 14]. The current results support the value of this measure during the
324 maintenance phase at 5 or more years after surgery. In this regard, although previous
325 investigators suggested nearly full recovery of knee muscle strength to deficits of within
326 10% at 5 or more years after surgery [20, 26], a finding supported by the current study when
327 looking at the group means, this did not undermine the value of measuring concentric force
328 production around the knee during such a relatively long follow-up. This is because large
329 inter-individual variabilities in the ability to produce powerful knee extension and flexion
330 torques characterized this population. Thus, close to perfect side-to-side symmetry of
331 concentric knee flexors and extensors torque was still associated with maintenance of higher
332 activity levels as opposed to subjects with either higher than (+)10% or lower than (-)10%
333 side-to-side symmetry indices. Altogether, it could be summarized that in order to maintain
334 higher activity levels at the maintenance phase after ACL reconstruction, patients would
335 benefit from reestablishment of concentric knee force production which is important during
336 jumping or changing directions, in addition to optimizing eccentric muscle torque around
337 the knee and hip which is important for the reestablishment of stable and effective landing.
338 Of note, drop jump landing kinematics in this study were reported through sagittal plane
339 motions at the hip, knee, and ankle although motion in this plane is inter-related with
340 coronal and transverse plane motions [25, 31]. Transverse plane kinematics involves smaller
341 range of motion and asymmetries and thus are harder to quantify compared to sagittal plane
342 kinematics [25]. Furthermore, accuracy of measuring coronal plane kinematics has been
343 previously questioned [27]. Therefore, the focus in this study was on sagittal plane
344 kinematics, which is also consistent with previous investigations [15].

345 Among the biomechanical measures tested, all showed side-to-side symmetry indices means
346 of within +/- 10% except hip torque at peak support moment which showed substantial

347 asymmetry with 17% higher values at the operated side. This may imply that patients
348 compensate for suboptimal knee function by generating higher torques at the hip region of
349 the involved side to dissipate the external loads during the drop jump landing. The clinical
350 significance of the hip role during this task is substantiated by the correlations between hip
351 torque levels at peak support moment during drop jump landing and both Tegner and Marx
352 scores at follow-up. It is also important to note that the clinical benefit of achieving
353 symmetry in this study should be viewed in light of the fact that the contralateral limb in this
354 group represented healthy uninjured limb with normal values of strength and kinematics.
355 Symmetry by itself may not be a desired goal in cases where the contralateral limb is poorly
356 functioning for whatever reason.

357 Preinjury Tegner activity level was associated with several biomechanical characteristics at
358 5 to 10 years after the operation. These variables accounted for 17% to 42% of the variance
359 of the Tegner preinjury scores in spite of the prolonged follow-up period. Five of the
360 variables were associated with preinjury activity for both the operated and the uninjured
361 limbs namely, isokinetic knee flexors and extensors torques, peak drop jump support
362 moment, knee torque during peak drop jump support moment and the single-legged hop
363 distance. These results may well exemplify a general association between preinjury activity
364 level and higher ability for force production, even in the long run. This also provides a
365 biomechanical explanation for the association observed previously [12] between preinjury-
366 and long-term follow-up Tegner levels after ACL reconstruction, beyond the mere "wish" of
367 any athlete to maintain activity levels throughout the years after an injury. Furthermore, in
368 the operated limb, the preinjury activity level was also associated with lower sagittal ROMs
369 during force absorption in all three lower extremity joints. Since knee sagittal ROM during
370 force attenuation was significantly related to Tegner score during follow-up as well,
371 together these results point again to a potential benefit of inclusion of an eccentric

372 strengthening of the lower musculature through a limited ROM in the adaptation process,
373 particularly with respect to the knee muscles. This perspective is in accordance with recent
374 meta-analyses that showed reductions in knee extension moments in ACL reconstructed
375 knees during single and double-legged landing tasks [15, 21], a finding which supports
376 addressing such deficits after surgery.

377 The significant relationships between Tegner activity level scores and long term movement
378 characteristics signify the relevancy of motion variables in the evaluation of the adaptation
379 process. Most strength measures of the operated limb as well as knee ROM correlated with
380 both preinjury and follow-up activity outcome measures. However, at follow-up, peak
381 support moment and hip and ankle ROM during drop jump, and single-legged hop distance
382 did not reach significance. On the other hand, hip torque during drop jump landing
383 significantly correlated with Tegner score at follow-up. The differences between the
384 preinjury and follow-up associations of activity level with movement variables can be, at
385 least in part, attributed to the span of the follow-up period. That is, at more than 5 years after
386 the operation, maintenance of activities is subjected to multiple factors that determine
387 whether athletes remain active and at which level. For example, factors that can affect
388 Tegner level at follow-up besides biomechanical constraints per-se may include changes in
389 life style for other reasons than the knee injury, accumulation of other health-related
390 problems, and other intervening factors [23, 29, 39]. With longer follow-up after surgery it
391 likely becomes even more challenging to isolate specific common biomechanical measures
392 which correlate with maintenance of active life style. This supports the rationale to limit this
393 type of a study, which focuses on biomechanical aspects of sport-related elements of
394 movement, to 5-to-10 years of follow-up, as opposed to studies which focus on the
395 development of specific long-term knee morbidity such as arthritis where longer follow-up
396 after ACL reconstruction is desired.

397 Limitations of this study include the retrospective design and using the uninjured leg after
398 an ACL injury as a reference for measuring neuromuscular deficits in the injured leg. This is
399 nevertheless in accordance with a recent study showing that neuromuscular functions which
400 included peak torque of knee extensors and flexors contractions measured on a Biodex
401 dynamometer, knee joint proprioception, one-leg standing balance test, and the single-
402 legged hop test for distance, were not impaired in the uninjured leg at more than six months
403 after an ACL injury despite the reduction in physical activity following an injury [43]
404 supporting that the contralateral limb can serve as adequate reference to examine recovery
405 of the injured leg's neuromuscular function during the rehabilitation process following an
406 injury [43]. In addition, the relatively limited follow-up rate of only 55% resulted from the
407 nature of this study which was a voluntary-based study requiring from the participants a
408 thorough time-consuming biomechanical evaluation in a biomechanical laboratory. In these
409 circumstances, 25 of the 55 patients, which were all young men from the workers class,
410 were unwilling to volunteer for personal reasons unrelated to the surgery. Despite this
411 limitation however, the study sample size was in accordance with previous investigations
412 that reported about hip and knee kinetics and kinematics after ACL reconstruction and
413 referred to sample sizes of between 11 and 35 patients [21].

414 **Conclusion**

415 At 5-to-10 years after ACL reconstruction, maintenance of sports participation is associated
416 with symmetric side-to-side concentric knee torques and with producing greater attenuation
417 of hip and knee ROM during drop jump landing in the operated limb. Therefore, eccentric
418 load programs which can improve attenuation phase kinematics during landing tasks may be
419 valuable in addition to traditional concentric training and facilitate enhanced long-term
420 outcomes.

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558 **Legends**

559 Table 1: Descriptive statistics of the patient activity reported outcomes

560 Table 2: Descriptive statistics of the biomechanical measures (mean \pm SD)

561 - Positive symmetry index indicates a higher value of the measured variable in the
562 contralateral uninjured limb and negative symmetry index indicates a higher value of the
563 measured variable in the operated limb

564 Table 3: Bi-variate correlation coefficients relating to the contralateral uninjured limb (CL),
565 the operated limb (ACLR), and the symmetry index between the limbs (SI) for the Tegner,
566 Marx, and IKDC scores

567 Table 4: Table 4: Bi-variate correlation coefficients relating to the contralateral uninjured
568 limb (CL), the operated limb (ACLR), and the symmetry index between the limbs (SI) for
569 the KOOS scores

570 *, $p \leq 0.05$; **, $p \leq 0.01$

571 †, total sagittal ROM = [hip ROM + knee ROM + ankle ROM]

572 GRF = Ground Reaction Force; BW = Body Weight; DJ = Drop Jump

573 - Significant correlations in bold

574 Table 5: Comparisons of the activity outcome scores between subgroups of symmetry
575 indices (SI) of knee torques and drop jump kinematics showing significant inter-
576 relationships

577 - The SI subgroup with the highest activity outcome score for each biomechanical
578 measure is indicated in bold

579 Figure 1: Correlations between knee side-to-side SIs of ROM during drop jump landing and
580 maintenance of sports participation as represented by KOOS-Sports sub-score

581 Figure 2: Correlations between hip side-to-side SIs of ROM during drop jump landing and
582 maintenance of sports participation as represented by KOOS-Sports sub-score